Artificial intelligence as a diagnostic tool for lung nodule evaluation

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Abstract: The clinical evaluation of lung nodules begins with an assessment of the probability that the nodule is malignant. The probability of malignancy can be estimated based on clinical experience or by using validated prediction models that incorporate known clinical and radiographic features associated with lung cancer. There has been a growing interest in the use of artificial intelligence (AI) to aid clinicians in performing this task. Advances in machine learning techniques have fostered progress in the development of automated systems with the goal to match or exceed the performance of clinicians. In this article we will review how lung nodules are currently evaluated, how AI may be used in lung nodule detection and classification, discuss its limitations, future directions and the necessary steps for its application in clinical practice.

Keywords: Lung nodule; lung cancer; machine learning; deep learning; artificial intelligence (AI)

Introduction

Lung nodules are radiographic opacities that are <30 mm in diameter, well-circumscribed, and surrounded completely by normal lung parenchyma. An opacity >30 mm is considered a lung mass (1). Lung nodules are typically detected on computed tomography (CT) scans of the chest performed for symptom evaluation (incidentally) or for lung cancer screening. Their clinical evaluation begins with an assessment of the probability that they are malignant (1). The earlier a lung cancer is detected, the higher the survival rates, however most nodules are not malignant. Thus, the goal of nodule management is to expedite the treatment of malignant nodules while minimizing testing for benign nodules (1,2).

The probability of malignancy can be estimated using clinical experience and intuition. It can also be assessed by using validated prediction models that incorporate known clinical and radiographic features associated with lung cancer (2). The accuracy of these methods is limited, resulting in difficult clinical decisions about how aggressively a lung nodule should be evaluated (2). Diagnostic molecular biomarkers are being studied as adjuncts to prediction methods, to assist with decision making (3). More recently there has been a growing interest in the use of artificial intelligence (AI) to aid clinicians in detecting and classifying lung nodules.

In this article we will review how lung nodules are currently evaluated, how AI has been studied in lung nodule detection and diagnosis, discuss its limitations, future directions and the necessary steps for its application in clinical practice.

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clinical practice.

**Lung nodule evaluation**

It is a challenge for a clinician to accurately diagnose a lung nodule. The first step is to assess the probability of malignancy (1). The clinical context within which the nodule is found is relevant. For example, a nodule found during the evaluation of a patient with a known cancer raises the suspicion for metastasis, and a nodule found incidentally in a young patient who never smoked cigarettes is likely benign. Clinicians estimate the probability that a nodule is malignant by taking into consideration clinical variables and imaging features that have been shown to be associated with lung cancer (1). The radiographic characteristics that have been independently associated with the likelihood of malignancy include nodule size, density, margin, evidence of growth, the presence of calcification, the presence of fat tissue, and cavitation (1). A clinician will incorporate these imaging features with clinical factors (age, smoking history, history of prior malignancies), and/or use validated clinical prediction models that include these features, to estimate the probability that the nodule is malignant (2,4). Table 1 summarizes the clinical and radiographic features included in validated prediction models.

The estimated probability that a nodule is malignant is used to guide management decisions. A probability of malignancy of 5% or less is considered very low risk, between 5% and 65% low to moderate risk and 65% or higher high risk (1). These risk groups are tied to management recommendations (1). Nodules that are classified at very low-risk for malignancy may require no further evaluation or just be followed with serial imaging to assess for growth. Nodules considered to have a high probability of malignancy should be considered for surgical resection, or for diagnostic testing to obtain a pathologic diagnosis. Nodules of low to moderate probability of malignancy are evaluated with additional testing, such as imaging with a fluoro-2-deoxy-D-glucose positron emission tomography (FDG-PET) scan, or by performing a non-surgical biopsy.

There are several limitations to the use of nodule risk prediction models in practice. First, it can be difficult to choose which model to apply as the populations from which the models were derived may not be representative of the

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**Table 1** Clinical and radiographic features included in validated prediction models

<table>
<thead>
<tr>
<th>Model</th>
<th>Predictors of malignancy</th>
<th>AUC</th>
</tr>
</thead>
<tbody>
<tr>
<td>Mayo Clinic (5)</td>
<td>Age, smoking history, history of extrathoracic cancer ≥5 years, nodule diameter, nodule</td>
<td>0.80</td>
</tr>
<tr>
<td></td>
<td>spiculation, upper lobe location</td>
<td></td>
</tr>
<tr>
<td>Veteran’s Affair (4)</td>
<td>Age, smoking history, time since quitting smoking, nodule diameter</td>
<td>0.79</td>
</tr>
<tr>
<td>Herder (6)</td>
<td>Mayo Clinic model and FDG-PET avidity intensity (none/faint/normal/ intense)</td>
<td>0.92</td>
</tr>
<tr>
<td>McWilliams/Tammemagi (Brock) (7)</td>
<td>Age, sex, family history of lung cancer, emphysema, nodule size, nodule type, nodule</td>
<td>0.94</td>
</tr>
<tr>
<td></td>
<td>location, nodule count</td>
<td></td>
</tr>
<tr>
<td>Gurney et al. (8,9)</td>
<td>Nodule spiculation, diameter and cavity wall thickness. Predictors of a benign etiology</td>
<td>0.87</td>
</tr>
<tr>
<td></td>
<td>were volume doubling time &gt;465 days and calcification.</td>
<td></td>
</tr>
<tr>
<td>Bayesian Inference Malignancy Calculator (BIMC) (10)</td>
<td>Age, smoking, history of previous malignancy, nodule diameter, edges, nodule location,</td>
<td>0.89</td>
</tr>
<tr>
<td></td>
<td>volume doubling time, minimum focal density, enhancement at contrast enhanced CT,</td>
<td></td>
</tr>
<tr>
<td></td>
<td>FDG-PET avidity</td>
<td></td>
</tr>
<tr>
<td>Thoracic Research Evaluation And Treatment (TREAT) (11)</td>
<td>Age, sex, BMI, FEV1, smoking history, hemoptysis, nodule size, nodule growth,</td>
<td>0.87</td>
</tr>
<tr>
<td></td>
<td>spiculation, nodule location, FDG-PET avidity</td>
<td></td>
</tr>
<tr>
<td>Peking University People’s Hospital (PKUPH) (12)</td>
<td>Age, nodule diameter, nodule border, nodule calcification, spiculation, family history</td>
<td>0.87</td>
</tr>
<tr>
<td></td>
<td>of cancer</td>
<td></td>
</tr>
<tr>
<td>Cleveland Clinic Model (13)</td>
<td>Age, smoking history, upper lobe location, solid and irregular/speculated edges,</td>
<td></td>
</tr>
<tr>
<td></td>
<td>emphysema, FDG-PET avidity, history of cancer other than lung</td>
<td></td>
</tr>
</tbody>
</table>

AUC, area under the curve; BMI, body mass index; CT, computed tomography; CXR, chest radiograph; FDG-PET, fluorodeoxyglucose-positron emission tomography; FEV1, forced expiratory volume in the first second; LDCT, low-dose CT; NR, not reported; PN, pulmonary nodule.
individual to whom they are applied. The accuracy of a prediction model is higher when it is applied in a population that is similar to that used to derive the model. It is not clear how these models perform in demographic minority groups as they are not well represented in the derivation studies. More important than the accuracy of the model outputs is the impact the estimate has on clinical decisions. Expert physician assessment of the probability of malignancy has variably been shown to be more accurate than nodule prediction models. However, physician management decisions may differ from guideline recommendations for the risk group that their patient falls in. One study showed the rate of lung resection in those with low risk nodules was the same as in those with high risk nodules (14).

**Artificial intelligence in lung nodule evaluation**

In health care, the largest impact of machine learning on big data has been in the field of diagnostic decision support. AI has been studied and implemented for many years in tasks such as computerized electrocardiogram analysis (15). Technological advances have led to growth in research on the use of AI-based systems in medical imaging. AI systems evolved to assist with workflow management, decision support, reader accuracy, or to supplement expertise in underserviced areas. Many imaging decision support tasks related to the management of lung nodules could be helped by AI systems.

Radiologists have found AI tools can help improve the efficiency of reading scans. Several studies have shown that nodule detection systems effectively help radiologists identify more nodules (16-18). Brown et al. studied the impact of implementing a commercial CT chest based computer-aided detection (CAD) system into the radiology workflow (18). The system provided automated detection and measurement of lung nodules, and it was integrated with a report dictation application. The authors reported reduced reading times by 7–44% compared to conventional manual methods (18).

The sophisticated and rapid analysis of large amounts of data has enabled greater knowledge of populations. The ultimate goal is to reduce cost and improve efficiency and quality of care by customizing population management interventions (19). Lung cancer screening is an area where AI can aid in population management due to challenges such as variability of lung cancer probability estimation between clinicians or radiologists, and high false-positive results (20-22).

**Deep learning techniques applied in nodule evaluation**

Deep learning techniques have already reached the field of lung nodule evaluation. The typical deep learning network involves feature extraction from the raw images and an objective function that learns the correlation between the features and the diagnosis. Instead of choosing features a priori, a set of training images and their target labels are provided to a deep learning network. The feature extraction portion usually consists of several layers of nonlinear processing units and transformation functions in addition to using conventional image processing operators such as filters. Convolutional Neural Network (CNN) techniques have become the most common pattern detection, segmentation and classification applications in the medical field. Unlike traditional clinical probability models, deep learning techniques build features from scratch rather than from a pre-selected set of features that rely on the contextual knowledge of the algorithm developer.

Fully automated systems using CNN have shown promising results in lung nodule detection. Huang et al demonstrated a fast and fully automated end-to-end system that can efficiently segment precise lung nodule contours from raw thoracic CT scans (23). The system had four components, including candidate nodule detection with “Faster regional”-CNN, candidate merging, false positive reduction, and nodule segmentation with CNN. The entire system had no human interaction or database specific design, and the average runtime was approximately 16 seconds per scan. The nodule detection accuracy was 91.4% with an average of 1 false positive per scan and 94.6% with an average of 4 false positives per scan. Pehrson et al. reviewed machine learning algorithms applied to the Lung Image Database Consortium Image Collection (LIDC-IDRI) database as a tool for the optimization of detecting lung nodules in thoracic CT scans. Their review showed that feature-based machine learning and deep learning algorithms can detect lung nodules with a high level of accuracy. Most feature-based algorithms achieved an accuracy >90%. The deep learning algorithms achieved an AUC in the range of 0.82–0.99 (24).

Recently, a deep learning algorithm with an end-to-end approach with both detection and lung cancer risk categorization tasks was used on cases from the National Lung Cancer Screening Trial (25). The proposed algorithm achieved an overall area under the curve of 94.4%, reduced false-positives by 11% and false-negatives by 5% compared to six radiologists.
Detection systems

Detection systems concentrate on the identification of suspicious lesions in chest images and alert radiologists to them. These systems are designed to improve sensitivity and accuracy in detection, while improving the efficiency of the radiologist by reducing the exam evaluation time. A good example of the potential application of a lung nodule detection system is in the setting of lung cancer screening, which can be a repetitive and difficult task for radiologists as they are often trying to detect small nodules.

Although they may have different structures, detection systems in general consist of 5 steps: image acquisition, preprocessing, lung segmentation, nodule detection and false positive reduction. Image acquisition is a process of acquiring medical images from imaging modalities. CT scans have been the most studied imaging modality. From a technical point of view, thin-section CT scans should be used when applying nodule detection systems. Lung segmentation improves the efficiency of nodule detection by extracting the lung volume from input CT images and removing the background and other irrelevant components. Many different methods have been used including optimal thresholding, rule-based region growing, global thresholding, 3-D-adaptive fuzzy thresholding, hybrid segmentation, and connected component labeling. After segmentation, the detection of areas suspicious of being a nodule can be done by multiple gray-level thresholding; shape- or template-matching-based morphological techniques or filtering-based methods. Detection of abnormalities that are not true nodules is common enough that a false-positive reduction step is necessary. This step involves feature extraction and nodule classification of “true nodules” and “non-nodules”.

Table 2 summarizes selected studies of lung nodule detection systems that reported sensitivity, specificity and false-positive rates. The overall sensitivity and specificity are high. They ranged from 85.9–100%, and 84–98.7%, respectively. The many different morphologies of nodules impact the false-positive rates. The detection systems need to identify nodules of different sizes and textures (solid, part solid, ground glass) in different locations (isolated, juxtapleural, perifissural or juxtavascular).

Nodule classification and cancer characterization

There are many examples of the successful use of machine

### Table 2 Selected studies of lung nodule detection systems

<table>
<thead>
<tr>
<th>Authors</th>
<th>Technique</th>
<th>Database</th>
<th>No of nodules</th>
<th>Sensitivity (%)</th>
<th>Specificity (%)</th>
<th>Average number false-positive/scan</th>
</tr>
</thead>
<tbody>
<tr>
<td>Naqi et al. (26)</td>
<td>Morphological operations, edge detection, bounding box, shape information</td>
<td>LIDC-IDRI</td>
<td>567</td>
<td>98.6</td>
<td>98.2</td>
<td>3.4</td>
</tr>
<tr>
<td>Saien et al. (27)</td>
<td>Sparse field level sets</td>
<td>LIDC-IDRI</td>
<td>198</td>
<td>83.9</td>
<td>90.7</td>
<td>3.9</td>
</tr>
<tr>
<td>Shaukat et al. (28)</td>
<td>Noise removal, segmentation by optimal thresholding, multiscale dot enhancement filtering, support vector machine</td>
<td>LIDC-IDRI</td>
<td>2,242</td>
<td>98.1</td>
<td>96</td>
<td>2.1</td>
</tr>
<tr>
<td>Liu et al. (29)</td>
<td>Fast segmentation method, random forest</td>
<td>LIDC</td>
<td>978</td>
<td>92.4</td>
<td>94.8</td>
<td>4.5</td>
</tr>
<tr>
<td>Javaid et al. (30)</td>
<td>K-means clustering, morphological filter</td>
<td>LIDC</td>
<td>133</td>
<td>91.6</td>
<td>96.7</td>
<td>3.1</td>
</tr>
<tr>
<td>Manikandan et al. (31)</td>
<td>Fuzzy auto-seed cluster means morphological algorithm</td>
<td>Private</td>
<td>801</td>
<td>100</td>
<td>93</td>
<td>0.38</td>
</tr>
<tr>
<td>Krishnamurthy et al. (32)</td>
<td>Morphological region-grow segmentation, edge bridge and fill technique</td>
<td>SPIE, AAPM, IDC</td>
<td>257</td>
<td>88</td>
<td>84</td>
<td>2</td>
</tr>
<tr>
<td>de Carvalho Filho et al. (33)</td>
<td>Extraction and reconstruction of the pulmonary parenchyma, nodule segmentation, support vector machine</td>
<td>LIDC-IDRI</td>
<td>182</td>
<td>85.9</td>
<td>97.7</td>
<td>1.8</td>
</tr>
<tr>
<td>Magalhaes et al. (34)</td>
<td>Growing neutral gas, 3D distance transform</td>
<td>LIDC</td>
<td>48</td>
<td>85.9</td>
<td>90.7</td>
<td>0.1</td>
</tr>
</tbody>
</table>

AAPM, American Association of Physicians in Medicine; LIDC-IDRI, Lung Image Database Consortium; NR, not reported; SPIE, International Society for Optics and Photonics.
learning techniques to classify and characterize lung nodules. Table 3 summarizes a selection of studies that used machine learning techniques for lung nodule classification. These studies applied defined feature-based algorithms as well as deep learning techniques; and different types of classifiers including CNN, fuzzy system, and support vector machine learning. They all show high accuracy with AUCs ranging from 87–99%. There is currently no agreement about the most efficient and effective methods (Table 1). Recent studies have compared AI systems with existing clinical prediction models and demonstrated that 2 different CNN models were able to classify lung nodule more accurately (41,42). Massion et al. trained a CNN model using scans from the National Lung Screening Trial, and its accuracy was compared with the Mayo and Brock clinical prediction models (5,7). The study showed that the deep learning system was more accurate in classifying low and high risk categories compared to the clinical models (41).

Hawkins et al. evaluated a cohort of patients with screen-detected lung cancer matched with a cohort of screening subjects with benign nodules. The authors identified 23 stable radiomic features that could predict nodules that would be found to be malignant 1 and 2 years later with accuracies of 80% and 79%, respectively (43). A few studies have demonstrated an association between radiomic features and the invasiveness of adenocarcinomas. Chae et al. differentiated part-solid nodules in pre-invasive and invasive adenocarcinoma using texture analysis with high accuracy (44). Maldonado et al. developed a computer-aided nodule assessment and risk yield (CANARY) system that builds a unique nodule radiomic signature that correlated well with the degree of tissue invasion and postsurgical patient outcomes (45).

Table 3: Selection of studies that used machine learning techniques for lung nodule classification

<table>
<thead>
<tr>
<th>Authors</th>
<th>Database</th>
<th>Features</th>
<th>Classifier</th>
<th>AUC</th>
</tr>
</thead>
<tbody>
<tr>
<td>Xie et al. (35)</td>
<td>LIDC-IDRI</td>
<td>Pre-selected, deep features</td>
<td>ANN</td>
<td>0.96</td>
</tr>
<tr>
<td>Xie et al. (36)</td>
<td>LIDC-IDRI</td>
<td>Pre-selected, deep features, 3D</td>
<td>CNN</td>
<td>0.95</td>
</tr>
<tr>
<td>Zhao et al. (37)</td>
<td>LIDC-IDRI</td>
<td>Deep features</td>
<td>CNN</td>
<td>0.87</td>
</tr>
<tr>
<td>Causey et al. (38)</td>
<td>LIDC-IDRI</td>
<td>Pre-selected, deep features, 3D</td>
<td>RF</td>
<td>0.99</td>
</tr>
<tr>
<td>Tajbakhsh et al. (39)</td>
<td>Private</td>
<td>Deep features</td>
<td>MTANN, CNN</td>
<td>0.88</td>
</tr>
<tr>
<td>Shen et al. (40)</td>
<td>LIDC-IDRI</td>
<td>Deep features, 3D</td>
<td>CNN</td>
<td>0.93</td>
</tr>
</tbody>
</table>

ANN, artificial neural network; AUC, area under the curve; CNN, convolutional neural network; LIDC-IDRI, Lung Image Database Consortium and Image Database Resource Initiative; MTANN, massive-training artificial neural networks; RF, random forest; SVM, support vector machines.

can be helpful in predicting gene expression profiling of non-small cell lung cancer (NSCLC). Liu et al. identified 11 radiomic features in peripheral lung adenocarcinomas that distinguished epidermal growth factor receptor (EGFR) mutant from wild types groups (46).

Advances in targeted therapies and immunotherapies have changed the paradigm for the diagnosis of lung cancer (47). The histologic confirmation of malignancy, or the simple differentiation of non-small cell carcinomas and small cell carcinomas, is no longer sufficient. Histologic subtyping, and molecular and genetic characterization are now standard of care as they help determine the most effective treatment (48). The identification of molecular and genetic markers requires invasive procedures to obtain an appropriate amount of tissue for testing. This process can be challenging, influenced by the general health of a patient and tumor location (48). It may prolong the time from diagnosis to treatment. Non-invasive methods to predict the presence of specific molecular and genetic markers may impact patient care. Since CT is routinely performed during lung cancer evaluation, there is an opportunity to assess imaging derived deep learning models as a non-invasive method for molecular characterization of a tumor. Wang et al. proposed a deep learning model to predict EGFR mutation status in lung adenocarcinoma using CT scans (49). An end-to-end deep learning model was used to predict the EGFR mutation status by CT scanning in 844 patients with lung adenocarcinoma. This model demonstrated an ability to differentiate EGFR-mutant and EGFR-wild type tumors (AUC 0.85 in the training cohort). Furthermore, this deep learning model showed higher accuracy than machine learning models based on hand-crafted CT features or clinical characteristics.
Challenges with the use of AI

Although AI has shown potential in lung nodule detection and classification, there are challenges that are worth discussing:

- **False-positives in nodule detection:** A major concern with the use of AI in lung nodule detection is the high prevalence of false-positive nodules due to their large variations in size, shape, and location on CT scans. False-positive reduction techniques are critical to distinguish true lung nodules from other structures that may look like nodules such as blood vessels, pleura, and atelectasis. False-positives may be a burden to the radiologist, lead to inaccurate judgments, and be a barrier to widespread use of detection systems. They may also cause emotional stress to patients, lead to unnecessary tests or procedures that carry their own risks, and increase the cost of care. Improvements in false-positive reduction techniques and the use of large public databases have helped mitigate this limitation (50).

- **Lack of reasoning:** The loss of “explainability” is one of the possible consequences of the use of AI for lung nodule classification. The malignancy prediction models that are currently used are mostly based on risk factors that are known to be associated with lung cancer and are connected to a biologic process so the reasoning is understandable. When AI is used, the patterns recognized are not necessarily associated with a biological process and no reasoning is provided for the output. It can also be challenging to change or remove an association that has already been made. This has several implications. For example, it may be difficult to explain to a patient who inquires why a nodule was classified as high risk by AI if a clinical prediction model calculator would classify it as low risk. A challenging question is whether clinicians and patients would follow the recommendation of a computer system when they cannot understand its reasoning.

- **Comprehensive evaluation of scans beyond nodules:** AI systems are typically focused on detecting and classifying nodules in the lung parenchyma. They do not include extra-pulmonary features that may be present in other locations such as the mediastinum and abdominal organs. For example, a lung nodule can be correctly classified as high probability for malignancy and the output recommendation could be a transthoracic needle biopsy or lung resection. However, the presence of mediastinal adenopathy would indicate consideration for a bronchoscopy with endobronchial ultrasound, or a concomitant liver lesion would indicate liver biopsy as the next step instead of a lung nodule biopsy.

- **Liability issues:** There are legal and ethical questions surrounding AI. Some of the questions related to the use of AI for lung nodule evaluation include who is ultimately responsible for its results and potential clinical recommendations, and whether the use of AI would require informed consent. AI in healthcare has not faced any major legal challenge but further research and understanding of the legal and ethical implications certainly need to be part of the process of bringing this technology to clinical practice.

- **The scarcity of labelled data:** Deep neural network architectures need to be trained on the entire image or larger sections of images. Creating ground truth for medical images consumes time and requires training. One large publicly accessible database of lung nodules was completed is the LIDC-IDRI which was a collaboration of seven academic centers and eight medical imaging companies (51). Each case required two-phase image annotation from four experienced thoracic radiologists. Even when the imaging data is adequate, finding an early stage malignant nodule in the CT scan is like finding a needle in the haystack. To develop a deep neural network that can find the needle requires many good signals in the training data set. This requires very large data sets, of which few are available.

- **Confidentiality of data:** An ideal deep learning model for lung nodule characterization would incorporate patient demographic, clinical, biomarker and radiographic features, as well as learn when it receives new data. To reach this point a large amount of patient data will be needed, bringing with it data storage security and patient privacy concerns.

Steps to implementation of AI systems in clinical practice

In April 2019, the Food and Drug Administration (FDA)
released a proposed regulatory framework for medical devices that use AI algorithms (52). The framework was issued for discussion purposes and it was not intended to be a guideline. The FDA is seeking industry feedback on the proposal with the goal of issuing a draft guideline in the future. The approach would allow the FDA’s regulatory oversight to take into consideration the nature of AI products while ensuring that its standards for safety and effectiveness are maintained. Last year, the FDA approved the first AI-based medical devices. One device is used for detecting retinopathy and the other for alerting providers of a potential stroke. However, the AI based products that the FDA cleared use “locked” algorithms that do not “learn” in real-time. The locked algorithms are modified by manufacturers on a periodic basis, which involves training the algorithm using new data and manual verification and validation of the updated algorithm. In contrast, “adaptive” algorithms do not need manual modification to learn and adapt. These algorithms learn from new user data through continuous use.

As any software is a medical device, products that use AI-based algorithms are expected to be assessed for their analytical and clinical validity. Analytical validation demonstrates that a specific device is suitable for its intended use by showing similar output when provided with similar input at separate times. Clinical validation demonstrates diagnostic accuracy, a measure of how well a test detects or predicts a clinical outcome. Despite analytical and clinical validation, clinical utility requires that clinicians and patients accept the AI-based algorithms for diagnosis and decision making, and that decisions based on the algorithms lead to more benefit than harm. The FDA clearance process is focused on the demonstration of safety and effectiveness. Although demonstration of clinical utility is not required in the proposed regulatory framework, it will be necessary for this technology to achieve wide acceptance in clinical practice. Successful demonstration of clinical utility involves developing sufficient evidence to demonstrate that a diagnostic test results in an improvement in patient outcomes. For example, a clinically useful AI system for lung nodule evaluation should help improve the balance of benefit to harm of diagnostic tests by leading to fewer lung cancer deaths, help expedite the treatment for early lung cancer, and help avoid unnecessary invasive procedures for benign nodules without delaying the diagnosis of malignant nodules. Other potential outcomes that would be considered clinically useful include improvement in the efficiency of care, compliance with care recommendations and cost-effectiveness.

Conclusions

AI systems may complement or augment traditional lung nodule evaluation. Deep learning algorithms are promising and expected to impact how lung nodules will be managed in the future. The application of these algorithms may assist with population management of nodules detected incidentally or by screening. Improvements in nodule characterization will aid in decision making about the need for additional diagnostic testing. Clinical utility remains to be proven—will patients and clinicians accept the AI conclusions without understanding how the conclusions were achieved, and will decisions be changed to the benefit of patients. Future advances need to be focused on perfecting the techniques, mitigating false-positive results, assessment of clinical utility, and how to best translate the results to patients.

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